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ARTICLE



Lattice Boltzmann phase field simulations of droplet slicing

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Abstract

We have performed two- and three-dimensional phase field simulations using the lattice-Boltzmann method of liquid drops rising through a continuous phase liquid under the influence of buoyancy. In their upward motion, the drops encounter a knife that is placed with the purpose of slicing the drops in two. A range of scenarios has been observed when the drop hits the knife and it has been investigated how the type of scenario depends on the dimensionless parameters governing the motion and slicing of the drop: the Eötvös number, the Morton number, and the ratio of the droplet size and the width of the knife. We studied symmetric and asymmetric encounters between drop and knife and kept track of the size distribution of the resulting fragments.

KEYWORDS

droplet slicing, free energy model, lattice Boltzmann method, rising droplet

1 | INTRODUCTION

Emulsions-systems of two or more immiscible liquids in the form of droplets dispersed in a continuous phaseare an essential part of many engineering processes and products. Controlling and influencing the drop sizes and drop size distributions often is essential for product quality and process efficiency. The desired direction of change of droplet size depends on our objectives. Increasing droplet size through coalescence could be helpful for gravity-driven phase separation as in oil-water separation devices.^[1-3] Reducing the droplet size increases interfacial area, which would benefit mass transfer between phases in, for instance, extraction operations.^[4,5] Another example is herbicide toxicity which will increase when its droplets get smaller, with smaller droplets creating a larger number of contact points on the plant compared to larger droplets.^[6]

In this paper we will be exploring size reduction of droplets by slicing them. Applications of slicing (or cutting) droplets are mainly found in microfluidics^[7]

and also-on a larger scale-in static mixers.^[8] Forte et al.^[9] investigated the fundamental mechanisms of oil droplet breakup in static mixers. They found that the drop size decreased to a critical point when the continuous phase (water) flow rate is increasing. It became difficult to reduce the oil drop size beyond the critical value. Additionally, Jaworski et al.^[10] modelled the process of droplet breakup in a static mixer and predicted the drop size evolution as a result of breakup. They found that intensive drop breakage occurred inside the inserts, resulting in a decrease of the average drop size. Ren et al.^[11] investigated the droplet breakup dynamics through a bi-layer bifurcating microchannel by numerical and experimental method. In the works cited above the drop motion is the result of a pressure driven flow, bounded by walls. In our paper, we study slicing of a freely rising drop in a periodic domain without bounding walls. This is a relatively simple system that, however, allows us to relate the starting point of our simulations (a rising drop) to be extensively available for drop rise velocities and drop shapes.^[12]

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Since the 1970s, a computational fluid dynamics (CFD) method based on solving the Reynolds-averaged Navier-Stokes (RANS) equation has been widely used for computing fluid flow and heat transfer.^[13] In the last 25 years, the lattice Boltzmann method (LBM) has been an efficient and powerful simulation method for various transport phenomena and processes,^[13-17] such as singlephase flow, multi-phase flows, turbulence, heat transfer, and phase change; it has also become a numerical tool to solve nonlinear partial differential equations.^[18-21] It has many unique benefits compared with other numerical methods.^[22] Unlike traditional methods, LBM is based on the perspective of micro-dynamics, taking macro physical quantities as the result of statistical averages of micro quantities. LBM has both microscopic and mesoscopic characteristics. It makes the interaction between particles easy to resolve and enables complex macroscopic phenomena of multiphase flow to appear naturally, thus providing an effective way to study the mechanism of multiphase flow under complex conditions.

There have been many studies using LBM to simulate droplet behaviour, including the droplet formation in micro-channels,^[16] deformation and breakup of a droplet exposed to a gas stream,^[23] three-dimensional (3D) binary droplet collisions,^[24] and so on. In addition to these, Zhou and Yu^[25] firstly addressed the dynamics of droplets in a static mixer using obstacles and porous media by means of a modified LBM. They found that there is a critical obstacle size, beyond which an obstacle is unfavourable for generating small droplets.

The behaviour of a droplet rising through liquid driven by buoyancy has been observed by experiment and numerical simulations. Bertakis et al.^[26] studied the binary liquid system (*n*-butanol/water) by experiment and numerical simulations. Watanabe and Ebihara^[27] used two-component two-phase LBM to simulate the process of drop rising. Komrakova et al.^[28] performed numerical simulation of n-butanol drop rising in water using the multiphase LBM, the simulation results they obtained agree well with the experimental data.

The focus of this study is the slicing of a rising droplet by a thin, flat plate—a knife. It is the aim of this study to investigate the feasibility of a knife as an efficient and controllable way of reducing the droplet size and to assist the design of process equipment for this purpose. We expect that the quality of the slicing process depends on the forces involved—buoyancy, surface, and viscous forces—as well as the geometrical details such as the sharpness and length of the knife. The diffuse interface free energy LBM model will be used. $^{\left[29\right]}$

2 | FLOW CONFIGURATION AND FLOW CONDITIONS

Numerical simulation of slicing a rising droplet is the focus of the present study. A liquid drop of density ρ_d and dynamic viscosity μ_d with equivalent diameter *d* is suspended in another liquid of density ρ_c and dynamic viscosity μ_c (subscripts *d* and *c* represent dispersed and continuous phase, respectively). The density difference between the two liquids is $\Delta \rho = \rho_c - \rho_d > 0$. The interfacial tension between the liquids is σ . At time t = 0, the drop is motionless. The droplet begins to rise driven by gravity and buoyancy and eventually attains a terminal rise velocity *u*. Table 1 gives the physical parameters for the binary benchmark system.

Along with gravitation acceleration *g*, the input parameters translate in four dimensionless groups that fully determine the problem. In this paper, we take for these dimensionless numbers the Eötvös number $Eo = \frac{g\Delta\rho d^2}{\sigma}$, the Morton number $Mo = \frac{g\Delta\rho \mu_c^2 \rho_c^2}{\sigma^3} = \frac{g\Delta\rho \mu_c^4}{\rho_c^2 \sigma^3}$, the density ratio $\lambda = \frac{\rho_d}{\rho_c}$, and the dynamic viscosity ratio $\eta = \frac{\mu_d}{\mu_c}$.

Dimensionless numbers that involve the rise velocity are output parameters: the Reynolds number $Re = \frac{ud\rho_c}{\mu_c}$, the Weber number $We = \frac{\rho_c u^2 d}{\sigma}$, and the Froude number $Fr = \frac{u^2}{gd}$. They characterize the relative importance of inertia over viscous effects (*Re*), inertia and surface forces (*We*), and inertia and gravity/buoyancy forces (*Fr*). Eo quantifies the ratio of gravity/buoyancy and surface forces. *Mo* is a constant for a given system; it does not contain the drop size.

An important reference point in our work is the diagram by Clift et al.^[12] that allows one to determine the Reynolds number (output parameter) as well as the drop shape and its rising regime (steady, wobbling, etc.) from *Eo* and *Mo* (input parameters).

We emphasize the importance of dimensionless numbers given that we use the LBM that is operated with its own lattice units with length and time units for the lattice spacing and time step, respectively. Translating between physical (SI) units and lattice units makes use of the dimensionless numbers; if a physical system and a numerical (LBM) system have the same input dimensionless numbers, they represent the same system. In this paper, parameters in lattice units will be given a ~. For example, the drop diameter in lattice units is denoted as \tilde{d} , which is the number of lattice spacings covered by the drop diameter. Unit conversion/scaling has been discussed in detail in Section 3.3. LU ET AL.

TABLE 1 Physical parameters for the simulated system

Density	$\rho_c = 1 \times 10^3 kg/m^3$
Density difference	$\Delta \rho = 1 \times 10^2 kg/m^3$
Dynamic viscosity	$\mu_c = 3.34 \times 10^{-3} Pa s$
Dynamic viscosity	$\mu_d = 3.34 \times 10^{-3} Pa s$
Surface tension	$\sigma = 1 \times 10^{-3} N/m$



FIGURE 1 Simulation domain with a knife at the top and the droplet released on the centre line

The base-case simulation domain was a cuboid of $20\tilde{d} \times 3\tilde{d} \times 1$ (for two-dimensional [2D] simulation) and $20\tilde{d} \times 3\tilde{d} \times 3\tilde{d}$ (for 3D simulation). As shown in Figure 1, the knife was placed at the top of the simulation domain. Initially it was located in the top-centre with the drop released on the centre line so that it was cut through the middle. Then the knife was moved laterally to study what happens if the drop hits the knife off-centre (see the details given in Section 5.2). Figure 1 also defines a Cartesian coordinate system as used throughout this paper.

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To complete the definition of the flow system, boundary conditions have to be specified. Periodic conditions applied on all outer faces. No-slip conditions were imposed on the knife, and we assume a 90° contact angle on the surface of the knife.

3 | SIMULATION METHOD

3.1 | Governing equations

In this study, we use the diffuse interface model for simulation of flow and interface dynamics. In diffuse interface (which are also called phase field) methods,^[30-32] we use a thin transition layer to represent the phase interface. An order parameter ϕ is used to describe the composition of the system. It is a function of position vector \mathbf{r} and time t. The value of ϕ is constant in the bulk phase of each fluid and varies continuously in the range [-1,1] over the thin interface.

Order parameter ϕ represents the relative concentration of the two components for the system when describing the behaviour of a binary system by phase field.^[33,34] Cahn and Hilliard^[34,35] proposed that continuity, momentum, and convection-diffusion equations can be used in combination for the simulation of fluid dynamics:

$$\partial_t \rho + \partial_\alpha (\rho u_\alpha) = 0 \tag{1a}$$

$$\partial_{t}(\rho u_{\alpha}) + \partial_{\beta}(\rho u_{\alpha}u_{\beta}) = -\partial_{\beta}P^{th}_{\alpha\beta} + \partial_{\beta}\nu(\rho\partial_{\alpha}u_{\beta} + \rho\partial_{\beta}u_{\alpha}) + g_{\alpha}\Delta\rho$$
(1b)

$$\partial_{t}\phi + \partial_{\alpha}(\phi u_{\alpha}) = M \partial_{\beta\beta}^{2} \mu \qquad (1c)$$

where ρ is density; ν is kinematic viscosity of the mixture; the index α stands for the Cartesian direction x, y, or z so that u_{α} is the velocity component in α direction; and g_{α} is the component of gravitational acceleration. The parameter M is the mobility parameter. Here, Pth is the thermodynamic pressure tensor, which contains two parts^[36]: an isotropic contribution $P\delta_{\alpha\beta}$ that describes the ideal gas pressure and the chemical pressure tensor $P^{\text{chem}}_{\alpha\beta}$ defined by the following:

$$P_{\alpha\beta}^{chem} = \delta_{\alpha\beta} \left(\phi \frac{\delta V}{\delta \phi} - V - \kappa \left(\phi \partial_{yy}^2 \phi + \frac{1}{2} |\partial_\alpha \phi|^2 \right) \right) + \kappa (\partial_\alpha \phi) \left(\partial_\beta \phi \right)$$
(2)

Phase separation is described by symmetrical double well potential; we can find this by the following:

$$V = \frac{A}{2}\phi^2 - \frac{A}{4}\phi^4 \tag{3}$$

The chemical potential $\mu(\phi)$ in Equation (1c) can be seen as follows^[37]:

$$\mu(\phi) = A\phi - A\phi^3 - \kappa \partial_{\alpha\alpha}^2 \phi \tag{4}$$

where A < 0, and both A and κ are parameters connected with surface tension and interface thickness as explained in Section 3.2.

Given the relatively minor density difference between continuous phase and disperse phase liquid (10%, see Table 1) we apply the Boussinesq approximation,^[38] which can be applied for flows with relatively small density differences. This means that the density in Equations (1a) and (1b) is uniform ($\rho = \rho_c$) and the density difference between drop and surroundings only has an effect in the forcing term $g_{\alpha}\Delta\rho$ in momentum Equation (1b).

3.2 | LBM implementation

The free energy model was proposed by Swift et al.^[29] to solve the system of Equation (1). This model is adopted in the present study. Two particle distribution functions are utilized: one function $f(\mathbf{r}, t)$ is used to solve the continuity Equation (1a)and the Navier-Stokes Equation (1b), and the second one $g(\mathbf{r}, t)$ is used for the convection-diffusion Equation (1c). The distribution functions evolve with discrete time steps Δt . All simulations were performed using a single relaxation time collision operator (known as Bhatnagar-Gross-Krook [BGK] model).^[39] The discretized LBEs are given as follows:

where index q is discretized velocity direction; $f_q(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t)$ and $g_q(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t)$ are postcollision particle distribution functions streamed from (r_α, t) to $(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t)$ along direction q; $f_q(r_\alpha, t)$ and $g_q(r_\alpha, t)$ represent pre-collision particle distribution functions; f_q^{eq} and g_q^{eq} are the discrete Maxwell–Boltzmann distributions (or equilibrium distributions); $c_{\alpha q}$ denotes the discrete velocity set and $c = \Delta x/\Delta t$ is the lattice speed; and τ_f and τ_g are dimensionless relaxation parameters. τ_f is determined by the kinematic viscosity, as follows:

$$\tau_f(\phi) = \frac{v(\phi)}{c_s^2 \Delta t} + \frac{1}{2} \tag{6}$$

where $c_s^2 = \frac{1}{3}$ represents the square of sound speed in lattice units.

The relationship between mobility M, coefficient of mobility Γ , and relaxation parameter τ_g is given by the following^[37]:

$$M = \Delta t \Gamma \left(\tau_g - \frac{1}{2} \right) \tag{7}$$

where the order parameter mobility *M* is determined by the parameter Γ as well as relaxation parameter τ_g . F_q is the forcing term.

The D3Q19 lattice is adopted here to discretize the velocity space.^[40] Each site has 19 velocity directions.

As noted above, the LBM works in dimensionless lattice units. We utilized uniform cubic lattices for the method described here. The mesh step Δx is unit of length, and the time step Δt is the unit of time. Here, we give the discrete velocity set:

$$f_q(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t) = f_q(r_\alpha, t) - \frac{f_q(r, t) - f_q^{eq}(r, t)}{\tau_f} + F_q$$
(5a)

The local density, local fluid momentum, and local order parameter of the fluid at lattice point are the results of summations over all directions q at that location, these can be seen as follows:

$$\sum_{q} f_{q} = \rho \tag{9a}$$

$$\sum_{q} \boldsymbol{c}_{q} \boldsymbol{f}_{q} = \rho \boldsymbol{u} + \frac{\Delta t}{2} \boldsymbol{F}$$
(9b)

$$\sum_{q} g_{q} = \phi \tag{9c}$$

The forcing term is incorporated as follows:

$$F_q = \omega_q \left(\boldsymbol{c}_q \cdot \boldsymbol{F} \right) \tag{10}$$

where F represents body force $\mathbf{g}\Delta\rho$ and ω_q are weight coefficients.^[41] Additional weighing coefficients $\omega_q^{\alpha\beta}$ are used for the equilibrium distributions; we can determine them by the following (see Equation (15)):

$$\omega_{0} = 1, \ \omega_{1-6} = \frac{1}{6}, \ \omega_{7-18} = \frac{1}{12}$$

$$\omega_{1-2}^{xx} = \omega_{3-4}^{yy} = \omega_{5-6}^{zz} = \frac{5}{12}, \ \omega_{3-6}^{yx} = \omega_{1-2,5-6}^{yy} = \omega_{1-4}^{zz} = -\frac{1}{3}$$

$$\omega_{7-10}^{xx} = \omega_{15-18}^{xx} = \omega_{7-14}^{yy} = \omega_{11-18}^{zz} = -\frac{1}{24}$$

$$\omega_{11-14}^{xx} = \omega_{15-18}^{yy} = \omega_{7-10}^{zz} = \frac{1}{12} \qquad (11)$$

$$\omega_{1-6}^{xy} = \omega_{1-6}^{yz} = 0, \ \omega_{7,10}^{xy} = \omega_{11,14}^{yz} = \omega_{15,18}^{zx} = \frac{1}{4}$$

 $\omega_{8-9}^{xy} = \omega_{12-13}^{yz} = \omega_{16-17}^{zx} = -\frac{1}{4}, \ \omega_{11-18}^{xy} = \omega_{7-10}^{yz} = \omega_{7-14}^{zx} = 0$

The full pressure tensor $P_{\alpha\beta}$ is defined by the following:

$$P_{\alpha\beta} = \sum_{q} f_{q} c_{q\alpha} c_{q\beta} \tag{12}$$

The equilibrium distributions must satisfy conditions (9) and ϕ is advected by fluid, which can be given by the following equation:

$$\sum_{q} g_q^{eq} c_{q\alpha} = \phi u_\alpha \tag{13}$$

The pressure tensor and chemical potential at equilibrium are as follows:

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$$\sum_{q} f_{q}^{eq} c_{q\alpha} c_{q\beta} = P_{\alpha\beta}^{th} + \rho u_{\alpha} u_{\beta}$$
(14a)

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$$\sum_{q} g_{q}^{eq} c_{q\alpha} c_{q\beta} = \Gamma \mu \delta_{\alpha\beta} + \phi u_{\alpha} u_{\beta}$$
(14b)

The equilibrium distributions^[41] f_q^{eq} and g_q^{eq} for populations $1 \le q \le 18$ are calculated using the following equations:

$$f_q^{eq} = \frac{\omega_q}{c^2} (p_0 - \kappa \phi \left(\partial_{xx}^2 \phi + \partial_{yy}^2 \phi + \partial_{zz}^2 \phi \right) + c_{aq} \rho u_a + \frac{3}{2c^2} \left(c_{aq} c_{\beta q} - \frac{c^2}{3} \delta_{\alpha \beta} \right) \rho u_a u_\beta + \frac{\kappa}{c^2} \left(\omega_q^{xx} \partial_x \phi \partial_x \phi + \omega_q^{yy} \partial_y \phi \partial_y \phi + \omega_q^{zz} \partial_z \phi \partial_z \phi \right) + \omega_q^{xy} \partial_x \phi \partial_y \phi + \omega_q^{xz} \partial_x \phi \partial_z \phi + \partial_y \phi \partial_z \phi)$$
(15)

$$g_q^{eq} = \frac{\omega_q}{c^2} \left(\Gamma \mu + c_{\alpha q} \rho u_\alpha + \frac{3}{2c^2} \left(c_{\alpha q} c_{\beta q} - \frac{3}{c^2} \delta_{\alpha \beta} \right) \phi u_\alpha u_\beta \right)$$
(16)

while the distributions for q = 0 are given by the following:

$$f_0^{eq} = \rho - \sum_{q=1}^{Q-1} f_q^{eq}$$
(17a)

$$g_0^{eq} = \phi - \sum_{q=1}^{Q-1} g_q^{eq}$$
 (17b)

The bulk pressure in Equation (15) obeys $p_0 = c_s^2 \rho + \frac{A}{2} \phi^2 - \frac{3A}{4} \phi^4$.

The kinematic viscosity v is related to ϕ , which can be seen as follows:

$$v(\phi) = v_c \frac{1-\phi}{2} + v_d \frac{1+\phi}{2}$$
 (18)

where v_c and v_d are kinematic viscosity of the continuous and dispersed phases, respectively. In this paper, $v_c = v_d$.

For a planar interface at x = 0, ϕ evolves over the interface as follows:

$$\phi(x) = tanh\frac{x}{\xi} \tag{19}$$

where $\phi = \pm 1$ is the value of ϕ in bulk phase at either side of the interface.

The width of diffuse interface ξ is given by the following^[37]:

$$\xi = \left(\frac{2\kappa}{-A}\right)^{1/2} \tag{20}$$

And the surface tension σ follows from Equation (21)^[37]:

$$\sigma = \frac{4}{3} \left(\frac{-A}{2k}\right)^{1/2} \tag{21}$$

We have to calculate the spatial gradients of ϕ to determine the equilibrium distributions. The stencils for gradients and Laplacian calculations are as follows^[41]:

$$\partial_{x} = \frac{1}{12\Delta x} \left[\begin{pmatrix} 0 & 0 & 0 \\ -1 & 0 & 1 \\ 0 & 0 & 0 \end{pmatrix}, \begin{pmatrix} -1 & 0 & 1 \\ -2 & 0 & 2 \\ -1 & 0 & 1 \end{pmatrix}, \begin{pmatrix} 0 & 0 & 0 \\ -1 & 0 & 1 \\ 0 & 0 & 0 \end{pmatrix} \right]$$
(22)
$$\nabla^{2} = \frac{1}{6\Delta x^{2}} \left[\begin{pmatrix} 0 & 1 & 0 \\ 1 & 2 & 1 \\ 0 & 1 & 0 \end{pmatrix}, \begin{pmatrix} 1 & 2 & 1 \\ 2 & -24 & 2 \\ 1 & 2 & 1 \end{pmatrix}, \begin{pmatrix} 0 & 1 & 0 \\ 1 & 2 & 1 \\ 0 & 1 & 0 \end{pmatrix} \right]$$
(23)

where the left, middle, and right matrices are the slices of the stencil when $z = \Delta x$, 0, and $-\Delta x$, respectively.

The discretized Equation (5) can be solved by two steps:

Collision step:
$$f'_q(r_\alpha, t) = f_q(r_\alpha, t) - \frac{1}{\tau_f} \left(f_q - f_q^{eq} \right) + F_q g'_q(r_\alpha, t)$$

= $g_q(r_\alpha, t) - \frac{1}{\tau_g} \left(g_q - g_q^{eq} \right)$
(24)

Streaming step:
$$f_q(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t) = f'_q(r_\alpha, t)$$

 $g_q(r_\alpha + c_{\alpha q}\Delta t, t + \Delta t) = g'_q(r_\alpha, t)$
(25)

3.3 | Scaling procedure

The LBM works in lattice space, which means the parameters should be translated into lattice units (lu). Scaling factors are utilized to realize it. In this work, the parameters with ~ represent those in lattice units. The scaling factor for surface tension can be written as follows:

$$C_{\sigma} = \frac{\sigma}{\tilde{\sigma}} \tag{26}$$

There are two numerical parameters related to surface tension, κ and A. The equation for κ is derived from Equation (21):

$$\kappa = \frac{3\xi}{4} \frac{\sigma}{C_{\sigma}} \tag{27}$$

In this work, the interface thickness ξ (see Equation (20)) was 1.14 lu for each simulation.^[36] The value of *A* can be calculated using Equation (20) once κ has been determined.

The density of liquid is $\tilde{\rho_c} = 1$ and we can obtain the density of droplet according to density ratio $\tilde{\rho_d} = \lambda \tilde{\rho_c}$.

Since the density difference is much smaller than actual densities of the liquids, the density differences only influence the forcing term $\Delta \rho g$ in Equation (1b). This is known as the Boussinesq approximation. The scaling factors for the forcing is based on the Eötvös number. According to the equation of *Eo*, the forcing term becomes the following:

$$\tilde{\Delta\rho g} = \frac{\tilde{\sigma}}{\tilde{d}^2} Eo \tag{28}$$

where d is the equivalent drop diameter.

In a similar way, based on the equation of *Mo* and η , the dynamic viscosity is defined as follows:

$$\tilde{\mu_c} = \left(\tilde{\rho}_c^2 \tilde{\sigma}^2 \tilde{d}^2 \frac{Mo}{Eo}\right)^{1/4} \tilde{\mu_d} = \eta \tilde{\mu_c}$$
(29)

And the kinematic viscosities are calculated by the following:

$$\tilde{\nu_c} = \frac{\tilde{\mu_c}}{\tilde{\rho_c}} \tilde{\nu_d} = \frac{\tilde{\mu_d}}{\tilde{\rho_d}}$$
(30)

From the above, the following scaling factors have been introduced and can be determined:

surface tension :
$$C_{\sigma} = \frac{\sigma}{\tilde{\sigma}};$$

density : $C_{\rho} = \frac{\rho}{\tilde{\rho}};$
kinematic viscosity : $C_{\nu} = \frac{\nu_c}{\tilde{\nu_c}};$ (31)
forcing : $C_{force} = \frac{\Delta \rho g}{\Delta \tilde{\rho} g}.$

Utilizing the equations of *Fr*, *Re*, and *We*, as well as the scaling factors (31), other scaling factors can be calculated as follows:

length :
$$C_d = \frac{C_{\nu}^2 C_{\rho}}{C_{\sigma}};$$

velocity : $C_u = \frac{C_{\sigma}}{C_{\nu} C_{\rho}};$ (32)
time : $C_t = \frac{C_{\nu}^3 C_{\rho}^2}{C_{\sigma}^2}.$

The other parameters can be translated from physical units into lattice units according to the scaling factors.

4 | VERIFICATION OF SIMULATIONS

The computer code for these simulations has been developed using FORTRAN 90. It is based on our previous study.^[42]

The objective of the present study is to investigate the behaviour of rising droplet being sliced by using the above-described LBM model. Several factors that may affect the process should be checked in advance. The results of a set of test simulations facilitated determining the suitable input parameters (*Eo*, *Mo*, λ , η) as well as the associated numerical settings. In this section, results of verification computations for domain



size, mesh resolution, and dimensionality (2D versus 3D) are presented.

4.1 | Domain size influence

We used fully periodic boundary conditions for describing a single drop moving through a large volume of fluid. We therefore need to make sure that the simulation domain is large enough so that the drop does not interact with itself and with the flow it creates over the periodic boundaries. On the other side, the domain size should be set reasonably to avoid excessive simulation time.

2D simulations of system with physical properties as given in Table 1 and drops of d = 1.0 mm were performed. The heights of the computational domain were set to 8*d* to 16*d* to determine the proper height. The width is equal to W = 3d, and D = 1 lu (2D simulations). All computations were performed with a drop diameter in lattice units of $\tilde{d} = 30$ lu. The simulation parameters (in lattice units) were determined according to the scaling procedure as outlined in Section 3.3 after it was established that the physical system has Eo = 1.0, $Mo = 1.24 \times 10^{-4}$, $\eta = 1$, and $\lambda = 0.90$.

The results are shown in Figure 2 in terms of the Reynolds numbers and the vertical locations towards reaching a steady speed.

The steady state Reynolds numbers reported in Figure 2A are within 0.2% of Re = 5.6, so that the impact of height on rising velocity can be negligible, which is consistent with the 3D simulation.^[28] The flow map due



FIGURE 2 The results for a d = 1.0 mm drop for different simulation domain heights in terms of the steady-state Reynolds number and rising distance. The domain width is 3*d*, and depth is 1 lu; Eo = 1.0 and $Mo = 1.24 \times 10^{-4}$. The dashed line in the left panel indicates the Reynolds number as derived from Clift et al.^[12]



FIGURE 3 The results for a d = 1.0 mm drop for different simulation domain widths in terms of the steady-state Reynolds number. The domain height is H = 10d, and depth is 1 lu (for 2D simulations) or W (for 3D simulations); Eo = 1.0 and $Mo = 1.24 \times 10^{-4}$. The horizontal dashed line indicates the Reynolds number as derived from Clift et al.^[12]

to Clift et al.^[12] indicates a Reynolds number of 5.0 for the specific values for *Eo* and *Mo*, where it should be noted that this map is based on (3D) experimental data.

The choice for the height *H* in the slicing simulations is mainly determined by the distance it takes for the drop to reach a steady speed. Figure 2B shows that this distance is approximately 2.16*d*. Because the drop is released at z > 0, and to ensure the drop behaviour has fully developed well before the drop hits the knife, a much larger domain height is used in the slicing simulations: H = 20d.

The verification simulations for the domain width were carried out in the range W = 2d - 10d. The other domain parameters are H = 10d, D = 1 lu (for 2D simulations,) or W = D = 2d - 5d (for 3D simulations). All computations were performed with drop diameter $\tilde{d} = 30$ lu.

From comparing Figures 2 and 3 it is clear that the width of the domain has a much stronger influence on the rise velocity than the domain height. In 3D the rise velocity becomes independent of the domain width beyond W = D = 4d. Since H = 8d in Figure 2, these results are also independent of domain height. The converged Reynolds number in the 3D results in Figure 3 is Re = 5.3 and is close to the Reynolds number Re = 5.0 that can be derived from the Clift et al.^[12] flow map.

Compared to the 3D results, the 2D results show a higher converged Reynolds number. This means the drag on a 2D (cylindrical) droplet is smaller than on a 3D (spherical) droplet. This has its analogy in flow around solid spheres and cylinders that for Re < 30 shows slightly smaller drag coefficients for cylinders than for spheres.



FIGURE 4 The results for a d = 1.0 mm drop for different drop diameter \tilde{d} in lattice space in terms of steady-state Reynolds number; Eo = 1.0 and $Mo = 1.24 \times 10^{-4}$

4.2 | Mesh resolution

The drop diameter \tilde{d} is a measure for the spatial resolution of the simulation and therefore has impact on the computational effort. It may play an important role in the accuracy of the result. For this we present results for a drop of d = 1 mm represented by $\tilde{d} = 20-60$ lu and with Eo = 1 and $Mo = 1.24 \times 10^{-4}$.

Changing the diameter in lattice units implies rescaling simulation parameters. The idea is to change the drop diameter \tilde{d} by a factor f_m ($\tilde{d}_2 = f_m \tilde{d}_1$). It is important to keep the dimensionless numbers constant, as well as viscosity and interface thickness: $\tilde{\mu_{c2}} = \tilde{\mu_{c1}}, \ \tilde{\mu_{d2}} = \tilde{\mu_{d1}}, \ \xi_2 = \xi_1$. The following relations make sure the Eötvös and Morton numbers are unchanged upon rescaling:

$$\frac{\tilde{\sigma}_2}{\tilde{\sigma}_1} = \frac{1}{f_m} \frac{\left(\Delta \tilde{\rho} g\right)_2}{\left(\Delta \tilde{\rho} g\right)_1} = \frac{1}{f_m^3} \frac{\kappa_2}{\kappa_1} = \frac{1}{f_m} \frac{A_2}{A_1} = \frac{1}{f_m}$$
(33)

The analysis was performed with simulations of 1.0-mm droplets with domain size $10\tilde{d} \times 3\tilde{d} \times 3\tilde{d}$ in 3D simulations and $10\tilde{d} \times 3\tilde{d} \times 1$ in 2D simulations. The resulting Reynolds numbers related to steady-state rise velocities are plotted in Figure 4. We observe good grid convergence behaviour for 2D as well as for 3D simulations. In the subsequent section on droplet slicing, a mesh resolution of $\tilde{d} = 30$ lu for 1-mm drops is adopted. In order to avoid extensive computations, 2D domains have been used in the simulation of droplets sliced by a knife. In Figures 3 and 4, we can see a reasonable

TABLE 2	Drop diameter a	l (mm) and	correspon	ding	Eo
number consi	dered in the pres	ent sir	nulat	ions		





FIGURE 5 The rising velocity of drops

agreement in terms of the Reynolds number based on the rise velocity between 2D and 3D.

With d = 30 lu (and d = 1 mm), the scaling factor of surface tension is $C_{\sigma} = 1.0 \text{ N/m}$. It gives the linear dimension scale factor $C_d = 3.33 \times 10^{-5}$ m and time scale factor $C_t = 4.66 \times 10^{-6}$ s.

5 | RESULTS

In this work, the parameters for simulated system are: $\lambda = 0.9$, $\eta = 1$, and $Mo = 1.24 \times 10^{-4}$; the values of *Eo* are different for different drop diameters (see Table 2). According to the diagram of Clift et al.,^[12] the drops are in the spherical (lower *Eo*) to ellipsoidal regime. Note that this diagram reflects a 3D situation.

5.1 | The knife is at the centre

The numerical simulations of slicing rising droplets have been carried out for d = 1.0-4.0-mm droplets, in order to observe the different slicing scenarios. For each

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droplet, the approach velocity, deformation, breakage, and slicing results have been analyzed. The approach velocity is the velocity at the moment the drop starts feeling the knife.

A range of scenarios has been observed when the drop hits the knife at centre, and it has been investigated how the type of scenario depends on the dimensionless parameters governing the motion and slicing of the drop (the Eötvös number, the ratio of the droplet size, and the width of knife).

The rising velocities for drops with diameter of 1.0–4.0 mm as a function of the vertical (*z*) location are depicted in Figure 5. The rising velocities of drops increase rapidly during the accelerating regime. Then, the 1.0- and 2.0-mm drops enter steady regimes. The velocity of a 1.0-mm drop decreases rapidly when it hits the knife and the drop finally stops moving. The knife hinders the 2.0-mm drop in rising, and finally slices the drop into two parts. A different behaviour is noticed for 3.0- and 4.0-mm drops; oscillations appear both for drop shapes (see Figure 6) and rising velocities (Figure 5) over the rising period. The acceleration period becomes longer with the increase of drop diameter. At the same time, the amplitude of velocity and shape oscillation becomes larger.

An increase in drop diameter results in obvious deformation in early times and leads to the oscillation behaviour of drop rising velocity. The drop shapes are presented in Figure 6 for 2.0-, 3.0-, and 4.0-mm drops. The drop deformations at the initial moment are different; at t = 0.1 s, the shapes of droplets are similar in the three cases, whereas, at t = 0.3 s, the drops deform in different ways. The 2.0-mm drop changes its shape to ellipse after deformation and maintains this shape until it touches the knife. At the same time, the larger drops (with diameter equals to 3.0 and 4.0 mm, respectively) get convex shapes, after which shape oscillations appear. The 4.0-mm drop develops two tails that then they break away and form two small satellite droplets. Surprisingly, during the ascent, they merge with the mother droplet again.

The approach velocity is related to drop diameter (see Figure 7). The aspect ratio *E*, which can be regarded as the ratio of the two principal axes of the droplet, is a description of the shape deformation quantitatively. E = 1 means that the droplet has a circular shape.^[43] According to Michaelides,^[43] the droplet is spherical if $E \ge 0.95$ (in this study, it is circular). Among the drop diameters involved in this study, only $d \le 1.5$ -mm drop can be considered having a circular shape when it hits the knife. Droplets with larger diameters are either deformed or oscillating. The drops with diameter $d \ge 1.8$ mm begin to deform, and $d \ge 2.8$ mm begin to oscillate

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<i>d</i> =2.0 mm	<i>d</i> =3.0 mm	<i>d</i> =4.0 mm
<i>t</i> =1.0 s	<i>t</i> =1.2 s	<i>t</i> =1.8 s
<i>t</i> =0.8 s	<i>t</i> =0.8 s	<i>t</i> =0.8 s
<i>t</i> =0.3 s	<i>t</i> =0.3 s	<i>t</i> =0.3 s
<i>t</i> =0.15 s	<i>t</i> =0.15 s	<i>t</i> =0.15 s
<i>t</i> =0.1 s	<i>t</i> =0.1 s	<i>t</i> =0.1 s
<i>t</i> =0.02 s	<i>t</i> =0.02 s	
		<i>i</i> -0.02 s

FIGURE 6 The shapes of 2D droplets of d = 2.0, 3.0, and 4.0 mm at different moments after being released at t = 0 and before hitting the knife

in shape and velocity. Besides, it is also found that the approach velocity for 1.8–2.6 mm gets reduced, which may be caused by deformation; the ellipse-shaped drops are subject to greater resistance due to their greater width.

The slicing behaviour is different for different drop sizes. The smallest droplet of d = 1.0 mm stops on the knife when sliced by knife, whether it is a sharp or a more obtuse knife (Figure 8A,B). Larger drops are easier to be sliced, and the slicing results do not depend much on the knife width (Figure 8C-G).

The effects of the relative sharpness of the knife s_r have been studied. It is defined as follows:

$$s_r = \frac{w_k}{d} \tag{34}$$

where w_k is the width of knife and *d* is the drop diameter. The simulated data are plotted in the graphical correlation in Figure 9.

Figure 9 shows the relationship between *Eo* and the relative thickness of the knife for $Mo = 1.24 \times 10^{-4}$. The results can be divided into three categories: (1) the droplet stops on the knife when sliced by relative blunt knife, which happens especially for smaller droplets (the lower *Eo* number); (2) the droplet passes the knife when it hits a sharp knife, and is not broken into two pieces; and

(3) the droplet is sliced into two parts for larger drop diameters / higher *Eo*.

The main conclusion of Figure 9 is that for a slicing process to be successful we need to overcome a threshold value of the Eötvös number of approximately Eo = 4. This critical value does not depend on the relative knife thickness, at least for $s_r < 0.1$.

5.2 | The knife is off-centre

In this section, the scenarios have been studied when the drops hit the knife off centre. The size of the simulation



FIGURE 7 Approach velocities as a function of drop diameters

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domain is $20\tilde{d} \times 3\tilde{d} \times 1$, and the relative thickness of the knife is in the range $s_r = 0.025 - 0.1$. The droplets are sliced into two unequal parts when the drop hits the knife off centre. The situations before and after slicing are presented in Figure 10.

In a range of off-centre distances, the volume ratios (given the 2D nature of the slicing simulations, the term volume ratio is actually a surface ratio, i.e., a ratio of volumes per unit length in the 3rd direction) for sliced drops increase with the deviation distances. Beyond this range, the drops also are sliced in two parts, but the smaller



FIGURE 9 Map of slicing scenarios with on the horizontal axis the relative thickness of the knife $(s_r = \frac{w_k}{d})$ and on the vertical axis the Eötvös number (*Eo*)



FIGURE 8 Slicing scenarios (A–G) as a function of drop size d and width of the knife w_k



FIGURE 10 Slicing in case the drop approaches the knife off-centre by a relative distance r/d as indicated



FIGURE 11 Ratio of the volume of the two drops formed after slicing as a function of the relative off-centre distance r/d. The dots represent individual simulations, the curves are quadratic fits (see Table 3)

droplet remains on the knife and cannot escape (Figure 10, $r/d \ge 5/12$ for d = 2.0 mm). We note in Figure 10 that under certain conditions the drops with d = 4.0 mm have developed satellites at the moment they interact with the knife.

The volume ratio of the two drops formed after slicing (the larger volume divided by the smaller volume) is a function of the relative off-centre distance r/d (see Figure 11). The data points correlate well according to a quadratic relationship as can also be seen in Figure 11. The coefficients of the fitting equations are **TABLE 3** The fitting equations between volume ratio (y) versus relative off-centre distance r/d (x) for different diameters d (mm)

<i>d</i> (mm)	Fitting equation	
2.0	$y = 8.32x^2 + 2.07x + 1.01$	(R2 = 0.9995)
3.0	$y = 11.59x^2 + 3.02x + 1.01$	(R2 = 0.9999)
4.0	$y = 1.11x^2 + 2.98x + 1.01$	(R2 = 0.9934)

shown in Table 3, along with the R^2 values that are all above 0.99.

As expected, the volume ratio monotonically increases with the off-centre distance. However, the trend with respect to the drop diameter is not monotonic. The largest volume ratios are found for d = 3 mm. Both d = 2 mm and d = 4 mm have smaller volume ratios for the same r/d values. This effect is related to the shape of the drops at the moment they start interacting with the knife.

6 | CONCLUSIONS

In this work, we performed numerical simulations of slicing a rising droplet in liquid. 2D and 3D simulations have been performed using a free energy LBM method. The proposed scaling procedure was utilized to translate the parameters into lattice units, which correspond to the physical units of the simulated system.

The simulation parameters such as simulation domain size, mesh resolution, and dimensionality

(2D versus 3D) were tested to verify the LBM model and computer code. In order to make sure that the drop does not interact with itself and with the flow it creates over the periodic boundaries, the domain width should be at least three drop diameters. The mesh resolution also plays an important role in the accuracy of results. A diameter $\tilde{d} = 30$ lu for 1 mm is the best choice because it satisfies both accuracy and simulation time. The results of 2D and 3D simulations were also compared. 2D slicing simulations have been adopted in order to avoid extensive computations.

We studied droplets with diameters of 1.0–4.0 mm, which were distributed in regions of circular, deformed, and oscillating. Our simulations captured shape deformation, rising velocity, and slicing results. The results of our numerical simulations (the rising velocity and Reynolds number) are consistent with the experimental data obtained by Clift et al.^[12]

A range of scenarios have been observed when the drop hits the knife at the centre as well as off-centre. Droplet slicing requires a threshold Eötvös number. Our simulations suggest it to be $Eo \approx 4$ if $Mo = 1.24 \times 10^{-4}$. This critical Eo was independent of the thickness of the knife as long as it was less than 0.1*d*. In case the drop hits the knife off-centre, the volume ratio of the two resulting fragments depends approximately quadratically on the off-centre distance.

It should be noted that the above conclusions are for a viscosity ratio of one and a density ratio close to one. We anticipate that the main effect of the density ratio is an effect on the rise velocity which, through the Eötvös number, impacts slicing. As for the viscosity ratio, its impact is likely to be more complex, in line with a former paper on the effect of the viscosity ratio of drop breakage as a result of shear.^[44]

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NOMENCLATURE

ρ	density (kg/m ³)
μ	dynamic viscosity (Pa s)
d	equivalent diameter (mm)
Δho	density difference (kg/m ³)
t	time (s)
σ	interfacial tension (N/m)
и	rising velocity (mm/s)
Eo	(dimensionless) Eötvös number
Мо	(dimensionless) Morton number
λ	density ratio
η	dynamic viscosity ratio
Re	(dimensionless) Reynolds number
We	(dimensionless) Weber number

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Fr	(dimensionless) Froude number
ϕ	order parameter of phase field
r	position vector (mm/s)
ν	kinematic viscosity (m ² /s)
gα	gravitational acceleration (m/s ²)
M	mobility parameter
Г	coefficient of mobility
$P^{th}_{\alpha\beta}$	thermodynamic pressure tensor (Pa)
$P_{\alpha\beta}^{\rm chem}$	chemical pressure tensor (Pa)
$P_{\alpha\beta}$	full pressure tensor (Pa)
$\mu(\phi)$	chemical potential (Pa)
<i>f</i> (<i>r</i> , <i>t</i>), g	particle distribution functions
(r , t)	
q	discretized velocity direction
f_{q}^{eq}, g_{q}^{eq}	discrete Maxwell-Boltzmann
1 -	(or equilibrium) distributions
$c_{\alpha q}$	discrete velocity (mm/s)
τ_f, τ_g	dimensionless relaxation parameters
A , κ	parameters connected with surface tension
	and interface thickness
c_s^2	speed of sound squared in lattice units (m^2/s^2)
F_q	forcing term ($F_q = g\Delta\rho$, N)
Δx	mesh step (mm)
Δt	time step (s)
ω_q	weight coefficients
p_0	bulk pressure (Pa)
ξ	diffuse interface (lu)
С	scaling factor
~	parameters in lattice units
\tilde{d}	equivalent drop diameter in lattice units (lu)
f_m	a factor (when changing the drop diameter d)
W	the weight of simulation domain (mm)
H	the height of simulation domain (mm)
D	the depth of simulation domain (mm)
E	aspect ratio of the droplet
w_k	width of the knife (mm)
Sr	the relative sharpness of the knife ($s_r = w_k/d$)
r	off-centre distance of the knife (mm)
r/d	relative off-centre distance

PEER REVIEW

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